ECG-BASED BIOMETRICS A Primer on Methods and Tools

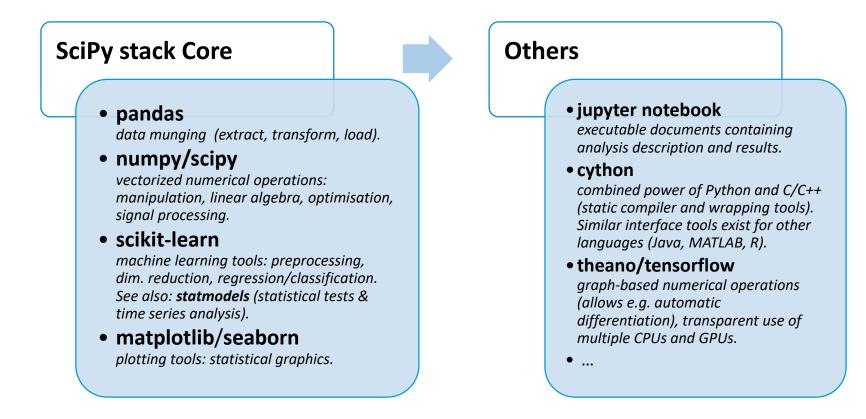
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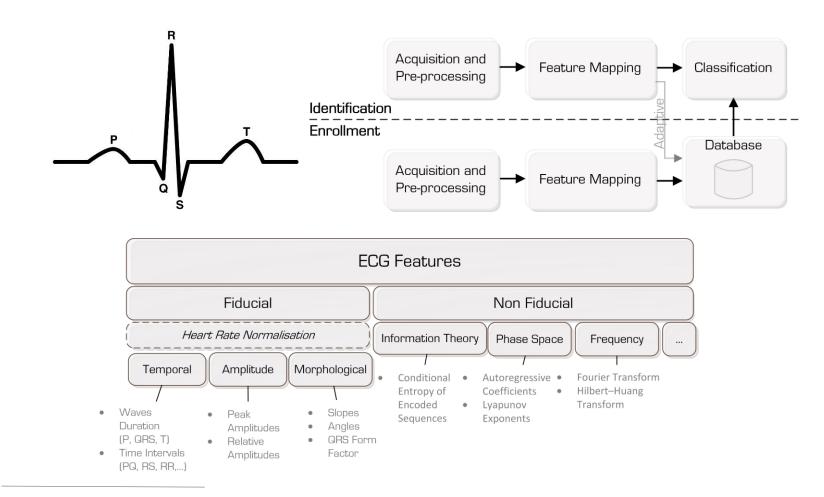
Preliminaries: Scientific Programming with Python

- Recommended Python 2.7 distribution
 - Anaconda: <u>https://www.continuum.io/downloads</u>
- Libraries/Modules (other than The Python Standard Library)



Check the corresponding module webpages and technical books published for instance by O'Reilly.

ECG-based Biometrics: Overview



 ECG biometrics surveys: (Odinaka, 2012) ECG Biometric Recognition: A Comparative Analysis. (Fratini, 2015) Individual Identification via Electrocardiogram Analysis.
 ECG analysis book: (Clifford, 2006) Advanced Methods and Tools for ECG Data Analysis.
 Physiologic signals & open-source software website: <u>http://physionet.org/</u>
 Machine Learning book: (Murphy, 2012) Machine Learning: A Probabilistic Perspective.

ECG-based Biometrics: Toolbox (I) (in development)

• Temporary location: PIANAS/Database/biometrics_code/

Overview:

This project aims to provide functions that should ease the process of setting up pattern recognition systems, namely those whose purpose is biometric identification based on ECG (Electrocardiogram).

- The Preprocessing folder contains functions that allow to create, plot and filter an ECG dataset.

- The Methods folder contains feature extraction and classification methods. In order to guarantee these functions share the same signature, wrappers.py has been created.

- The module main.py implements the pipeline that consists of data selection, feature extraction, classification and logging. To create the filtered datasets, the preprocessing step has to be run beforehand.

- For more information, check the corresponding modules.

Other Notes:

To use the <u>autoencoder</u>, theano and keras (<u>https://keras.io/)</u> must be installed. Installing these on Linux shouldn't offer any complications. However, if one wants to use Windows, this tutorial should be followed (it should also work for win7/8): <u>https://github.com/philferriere/dlwin.</u>

Python version:

2.7

Python packages:

scipy stack - https://www.scipy.org/install.html

scikit-learn - http://scikit-learn.org/stable/documentation.html

theano - http://deeplearning.net/software/theano/

keras - https://keras.io/

pywavelets - https://pywavelets.readthedocs.io/en/latest/

seaborn - http://seaborn.pydata.org/

joblib - https://pythonhosted.org/joblib/parallel.html

matlab - https://www.mathworks.com/help/matlab/matlab_external/install-the-matlab-engine-for-python.html
 (Requires R2014b or later)

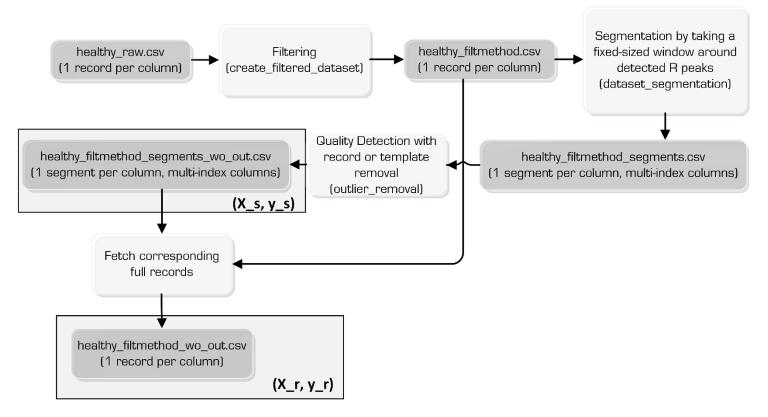
Version requirements:

scipy: >=0.18

scikit-learn: >=0.18

ECG-based Biometrics: Toolbox (II) (in development)

• **Preprocessing pipeline** (heartbeat-based quality detection)

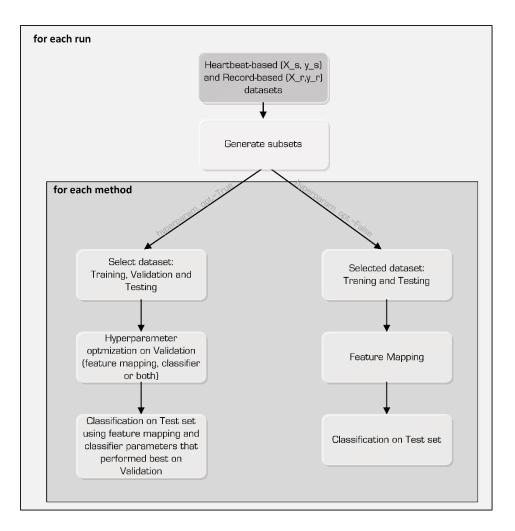


• **Preprocessing pipeline** (record-based quality detection): does not require segmentation beforehand.¹

¹ For instance, UNSW quality detection: (Khamis, 2016) QRS Detection Algorithm for Telehealth Electrocardiogram Recordings .

ECG-based Biometrics: Toolbox (III) (in development)

• Pattern recognition pipeline



ECG-based Biometrics: Toolbox (IV) (in development)

All feature extraction methods have the option of truncation and resampling of data arguments (this is accomplished with a function decorator).

Feature Extraction (FE):
Baseline (with option of dimensionality reduction: + DCT/LDA/PCA/KPCA)
Autocorrelation (+ DCT/LDA/PCA/KPCA) [1][2][3]
Short-Time Fourier Transform (stft) [4]
Wavelet decomposition (wt) [5]
Autoencoder (Shallow or Deep) [6]

Classifiers: kNN (works with all FE methods)

Classifier/Stand-alone system (to use these select baseline with no dimensionality reduction as feature extraction and the following as classifiers): Time-Frequency Robust Feature Selection (clf_tf_rbfs) [4] Wavelets with measures 'prd', 'ccorr', 'wdist' (clf_wavelet) [5] Phase representation with measures 'nSC', 'MNPD', 'MNPM' (clf_rec_phase) [7]

PCA: Principal Component Analysis KPCA: Kernel PCA LDA: Linear Discriminant Analysis DCT: Discrete Cosine Transform

[1] (Plataniotis, 2006) ECG biometric recognition without fiducial detection.

[2] (Agrafioti, 2008) ECG Based Recognition Using Second Order Statistics.

[3] (Hejazi, 2016) ECG biometric authentication based on non-fiducial approach using kernel methods.

[4] (Odinaka, 2010) ECG biometrics A robust short-time frequency analysis.

[5] (Chan, 2008) Wavelet distance measure for person identification using electrocardiograms.

[6] (A. Eduardo, 2017) ECG-based Biometrics using a Deep Autoencoder for Feature Learning.

[7] (Fang, 2013) QRS detection-free electrocardiogram biometrics in the reconstructed phase space.

(show a notebook with some results)

Phase-wrapped ECG

1. R peak detection

2. Phase assignment

- 1. Generate linear ramp from 0 to 2π for each RR segment
- 2. Subtract 2π where $\theta \ge \pi \rightarrow$ each heartbeat in $[-\pi, \pi[$

3. Binarisation

- 1. Split each heartbeat according to a given number of bins
- 2. Take the mean amplitude and phase for each bin (alternatively, median/other sample statistic)

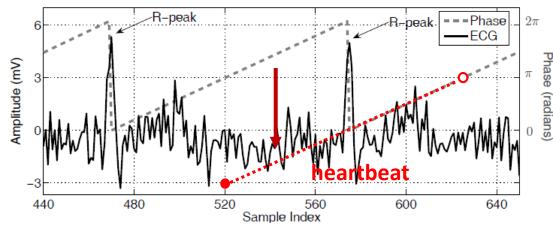


Fig. 1. An illustration of the phase assignment approach

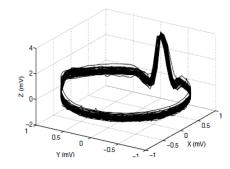


Fig. 2. Several cycles of the ECG phase-wrapped in the state space

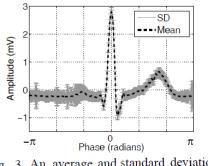


Fig. 3. An average and standard deviation-bar of 30 ECG cycles of a noisy ECG

• A similar procedure can be applied to other quasi-periodic signals (e.g. BVP) using the most easily-detectable fiducial event!

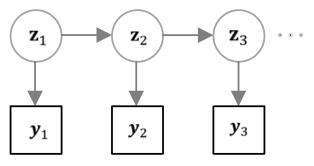
⁽Sameni, 2007) A Nonlinear Bayesian Filtering Framework for ECG Denoising. The Open-Source Electrophysiological Toolbox (OSET) - MATLAB: http://www.oset.ir/

State Space Models: Overview (I)

• Generic form:

$$\mathbf{z}_t = g(\mathbf{u}_t, \mathbf{z}_{t-1}, \boldsymbol{\epsilon}_t)$$
$$\mathbf{y}_t = h(\mathbf{z}_t, \mathbf{u}_t, \boldsymbol{\delta}_t)$$

- \mathbf{Z}_t : hidden state
- \mathbf{u}_t : (optional) control signal
- **y**_t: observation
- g: transition model
- *h*: observation model
- $\boldsymbol{\epsilon}_t$: system noise at time t
- $oldsymbol{\delta}_t$: observation noise at time t
- **Graphical representation:** (identical to Hidden Markov Model, states are now continuous)



• Notable special case: linear-gaussian SSM (LG-SSM) or linear dynamical system (LDS)

$$\mathbf{z}_t = \mathbf{A}_t \mathbf{z}_{t-1} + \mathbf{B}_t \mathbf{u}_t + \boldsymbol{\epsilon}_t \qquad \boldsymbol{\epsilon}_t \sim \mathcal{N}(\mathbf{0}, \mathbf{Q}_t)$$

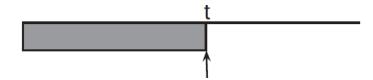
$$\mathbf{y}_t = \mathbf{C}_t \mathbf{z}_t + \mathbf{D}_t \mathbf{u}_t + \boldsymbol{\delta}_t \quad \boldsymbol{\delta}_t \sim \mathcal{N}(\mathbf{0}, \mathbf{R}_t)$$

• Supports exact inference: if inital state is Gaussian, all subsequent states are Gaussian.

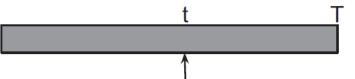
⁽Murphy, 2012) Machine Learning: A Probabilistic Perspective.

State Space Models: Overview (II)

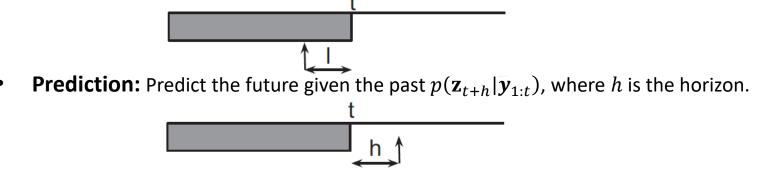
- Types of inference problems for time series:
 - **Filtering:** Compute belief state $p(\mathbf{z}_t | \mathbf{y}_{1:t})$ online as the data streams in.



• Offline Smoothing: Compute $p(\mathbf{z}_t | \mathbf{y}_{1:T})$ offline, given all evidence. Uncertainty is reduced by incorporating all future observations.



• **Fixed lag Smoothing:** Compromise between online and offline estimation. Compute $p(\mathbf{z}_{t-l}|\mathbf{y}_{1:t})$, with l > 0 being the lag. Better performance than filtering, but at the cost of a slight delay.



State Space Models: Overview (III)

• If the model is a LG-SSM, Kalman filter is the algorithm for exact filtering

 $p(\mathbf{z}_t | \mathbf{y}_{1:t}, \mathbf{u}_{1:t}) = \mathcal{N}(\mathbf{z}_t | \boldsymbol{\mu}_t, \boldsymbol{\Sigma}_t)$

• Prediction step:

$$p(\mathbf{z}_{t}|\mathbf{y}_{1:t-1}, \mathbf{u}_{1:t}) = \int \mathcal{N}(\mathbf{z}_{t}|\mathbf{A}_{t}\mathbf{z}_{t-1} + \mathbf{B}_{t}\mathbf{u}_{t}, \mathbf{Q}_{t})\mathcal{N}(\mathbf{z}_{t-1}|\boldsymbol{\mu}_{t-1}, \boldsymbol{\Sigma}_{t-1})d\mathbf{z}_{t-1}$$

$$= \mathcal{N}(\mathbf{z}_{t}|\boldsymbol{\mu}_{t|t-1}, \boldsymbol{\Sigma}_{t|t-1})$$

$$\boldsymbol{\mu}_{t|t-1} \triangleq \mathbf{A}_{t}\boldsymbol{\mu}_{t-1} + \mathbf{B}_{t}\mathbf{u}_{t}$$

$$\boldsymbol{\Sigma}_{t|t-1} \triangleq \mathbf{A}_{t}\boldsymbol{\Sigma}_{t-1}\mathbf{A}_{t}^{T} + \mathbf{Q}_{t}$$

• Measurement step (after receiving observation y_t):

 $p(\mathbf{z}_t|\mathbf{y}_t, \mathbf{y}_{1:t-1}, \mathbf{u}_{1:t}) \propto p(\mathbf{y}_t|\mathbf{z}_t, \mathbf{u}_t) p(\mathbf{z}_t|\mathbf{y}_{1:t-1}, \mathbf{u}_{1:t})$ Residual

$$p(\mathbf{z}_t | \mathbf{y}_{1:t}, \mathbf{u}_t) = \mathcal{N}(\mathbf{z}_t | \boldsymbol{\mu}_t, \boldsymbol{\Sigma}_t)$$

$$\boldsymbol{\mu}_t = \boldsymbol{\mu}_{t|t-1} + \mathbf{K}_t \mathbf{r}_t$$

$$\boldsymbol{\Sigma}_t = (\mathbf{I} - \mathbf{K}_t \mathbf{C}_t) \boldsymbol{\Sigma}_{t|t-1}$$

Correction term: the amount of weight placed on the error depends on the gain

If $\mathbf{C}_t = \mathbf{I} \rightarrow \mathbf{K}_t = \mathbf{\Sigma}_{t|t-1} \mathbf{S}_t^{-1}$: ratio of prior and measure error covariances.

E.g. strong prior or noisy sensors $\rightarrow |\mathbf{K}_t|$ is small.

Residual (*diff. between observed and predicted*)

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ŵ.

$$\begin{aligned} \hat{\mathbf{y}}_t &\stackrel{=}{=} & \mathbb{E}\left[\mathbf{y}_t | \mathbf{y}_{1:t-1}, \mathbf{u}_{1:t}\right] = \mathbf{C}_t \boldsymbol{\mu}_{t|t-1} + \mathbf{D}_t \mathbf{u}_t \\ \hat{\mathbf{x}}_t &\stackrel{=}{=} & \mathbb{E}\left[\mathbf{y}_t | \mathbf{y}_{1:t-1}, \mathbf{u}_{1:t}\right] = \mathbf{C}_t \boldsymbol{\mu}_{t|t-1} + \mathbf{D}_t \mathbf{u}_t \\ \mathbf{x}_t &\stackrel{=}{=} & \boldsymbol{\Sigma}_{t|t-1} \mathbf{C}_t^T \mathbf{S}_t^{-1} \\ \mathbf{x}_t &\stackrel{=}{=} & \boldsymbol{\Sigma}_{t|t-1} \mathbf{C}_t^T \mathbf{S}_t^{-1} \\ \mathbf{x}_t &\stackrel{=}{=} & \mathbf{x}_t [(\mathbf{C}_t \mathbf{z}_t + \boldsymbol{\delta}_t - \hat{\mathbf{y}}_t) (\mathbf{C}_t \mathbf{z}_t + \boldsymbol{\delta}_t - \hat{\mathbf{y}}_t)^T | \mathbf{y}_{1:t-1}, \mathbf{u}_{1:t}] \\ &= & \mathbb{E}\left[(\mathbf{C}_t \mathbf{z}_t + \boldsymbol{\delta}_t - \hat{\mathbf{y}}_t) (\mathbf{C}_t \mathbf{z}_t + \boldsymbol{\delta}_t - \hat{\mathbf{y}}_t)^T | \mathbf{y}_{1:t-1}, \mathbf{u}_{1:t}] \end{aligned}$$

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State Space Models: Overview (IV)

- There is also a very efficient smoother for LG-SSM: *Rauch-Tung-Striebel (RTS) smoother* aka *Kalman smoothing* algorithm. Kalman filter performs the forward pass and the smoother performs the backward pass (using information from the forward pass). This is related to message passing in graphical models.
- What if the model is not linear in the parameters? Approximate Inference. For instance, <u>Extended Kalman Filter (EKF)</u>: linearise g and h about the previous state estimate using a first order Taylor series expansion and then apply the standard Kalman filter equations. The same applies to the smoother.

$$\begin{aligned} \mathbf{z}_t &= g(\mathbf{u}_t, \mathbf{z}_{t-1}) + \mathcal{N}(\mathbf{0}, \mathbf{Q}_t) \\ \mathbf{y}_t &= h(\mathbf{z}_t) + \mathcal{N}(\mathbf{0}, \mathbf{R}_t) \end{aligned}$$

Approximate system model:

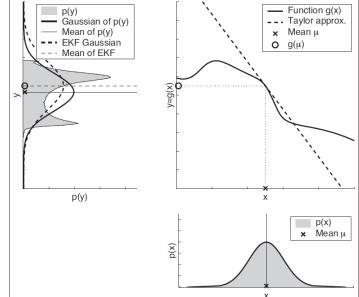
$$p(\mathbf{z}_t | \mathbf{z}_{t-1}, \mathbf{u}_t) \approx \mathcal{N}(\mathbf{z}_t | \mathbf{g}(\mathbf{u}_t, \boldsymbol{\mu}_{t-1}) + \mathbf{G}_t(\mathbf{z}_{t-1} - \boldsymbol{\mu}_{t-1}), \mathbf{Q}_t)$$

$$G_{ij}(\mathbf{u}) \triangleq \frac{\partial g_i(\mathbf{u}, \mathbf{z})}{\partial z_j}$$

$$\mathbf{G}_t \triangleq \mathbf{G}(\mathbf{u}_t)|_{\mathbf{z}=\boldsymbol{\mu}_{t-1}}$$

Approximate measurement model:

$$p(\mathbf{y}_t | \mathbf{z}_t) \approx \mathcal{N}(\mathbf{y}_t | \mathbf{h}(\boldsymbol{\mu}_{t|t-1}) + \mathbf{H}_t(\mathbf{z}_t - \boldsymbol{\mu}_{t|t-1}), \mathbf{R}_t)$$
$$H_{ij} \triangleq \frac{\partial h_i(\mathbf{z})}{\partial z_j}$$
$$\mathbf{H}_t \triangleq \mathbf{H}_{|\mathbf{z} = \boldsymbol{\mu}_{t|t-1}}$$



<u>Unscented Kalman Filter (UKF)</u>: Instead of a linear approximation, pass a deterministically set of points (sigma points) through the function and fit a Gaussian to the resulting transformed points.

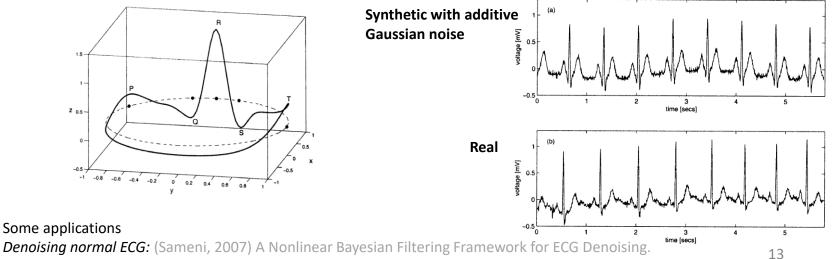
ECG Dynamical Model: Overview

- (McSharry, 2003) A Dynamical Model for Generating Synthetic Electrocardiogram ٠ Signals
 - Set of differential equations that generates a trajectory in a space with coordinates (x, y, z):

$$\begin{cases} \dot{x} = \gamma x - \omega y \\ \dot{y} = \gamma y + \omega x \qquad \text{Sum of Gaussian kernels} \\ \dot{z} = -\sum_{i \in \{P,Q,R,S,T\}} a_i \Delta \theta_i \exp\left(-\frac{\Delta \theta_i^2}{2b_i^2}\right) - (z - z_0) \qquad \text{Baseline wander term } (z_0 \text{ is a low sinusoidal component}) \end{cases}$$

$$\gamma = 1 - \sqrt{x^2 + y^2}, \Delta \theta_i = (\theta - \theta_i) \mod 2\pi, \ \theta = atan2 \ (v, x)$$

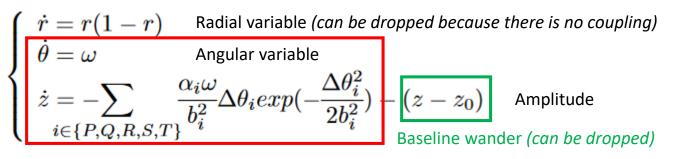
 $\omega = 2\pi f$ Angular velocity of the trajectory (related to the beat-to-beat frequency)



Attacking Biometric Systems: (Eberz, 2017) Broken Hearted: How to Attack ECG Biometrics.

ECG Dynamical Model: Denoising (I)

- (Sameni, 2007) A Nonlinear Bayesian Filtering Framework for ECG Denoising
 - Modification of the state equations to polar coordinates:



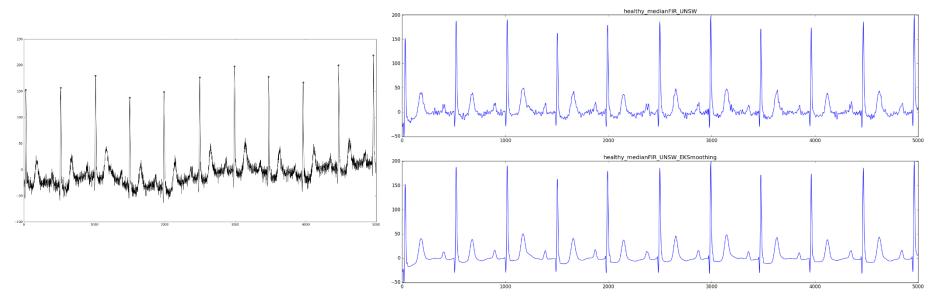
- Discrete form: $\begin{cases}
 \theta_{k+1} = (\theta_k + \omega \delta \mod(2\pi)) \\
 z_{k+1} = -\sum_i \delta \frac{\alpha_i \omega}{b_i^2} \Delta \theta_i exp(-\frac{\Delta \theta_i^2}{2b_i^2}) + z_k + \eta \quad \text{Random additive noise} \\
 \Delta \theta_i = (\theta_k - \theta_i) \mod(2\pi).
 \end{cases}$
- How to denoise (simplified):
 - 1. Compute the phase-wrapped ECG mean and standard deviation.
 - 2. Nonlinear least squares optimisation to determine the parameters (amplitude, angular width and position of PQRST waves): α_i , b_i , θ_i .
 - 3. Linearisation of the model, Kalman filter followed by the Kalman smoother equations.
- In this model, the parameters α_i , b_i , θ_i are fixed, but it is possible to augment the state equations to introduce variability:

(Su, 2013) [Master Thesis] ECG Noise Filtering Using Online Model-Based Bayesian Filtering Techniques.

ECG Dynamical Model: Denoising (II)

(Sameni, 2007) A Nonlinear Bayesian Filtering Framework for ECG Denoising

- Other quasi-periodic signals can be modelled using a similar framework (e.g. BVP, PCG): (Almasi, 2011) A dynamical model for generating synthetic Phonocardiogram signals.
- Denoising on data from Hospital Santa Marta DBCarlos, subject 2016 (lead I):



Popular alternatives are based on Empirical Mode Decomposition (intrinsic mode function rejection) and ٠ Wavelet Transform (coefficient thresholding/shrinkage): e.g.

(Kabir, 2012) Denoising of ECG signals based on noise reduction algorithms in EMD and wavelet domains.

Other observations: Some papers on denoising only consider white noise. Real noise spectrum can be colored and noise samples are often correlated in time – see (Sameni, 2007).

ECG Dynamical Model: Spoofing Attack (I)

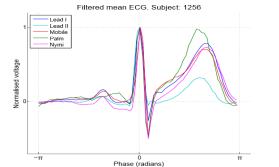
- How to impersonate a legitimate user in ECG Biometrics? We could generate synthetic ECGs using a dynamical model where parameters are extracted from previous measurements.
- (Eberz, 2017) Heart Broken: How to Attack ECG Biometrics
 - <u>Signal injection methods</u>: HW waveform generator, laptop soundcard with SW-based waveform generator, playback of .wav-encoded ECG signal.



• Other considerations:

Attacker takes photo from the victim's ECG \rightarrow image analysis Source device \neq target device (nymi band) $\rightarrow \neq$ waveform morphology among devices





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ECG Dynamical Model: Spoofing Attack (II)

- (Eberz, 2017) Heart Broken: How to Attack ECG Biometrics
 - Training cross-device mapping and generation of attack signals:

